Иммунохимические методы детекции

TABLE 6-1

Forward and reverse rate constants (k_1 and k_{-1}) and association and dissociation constants (K_a and K_d) for three ligand-antibody interactions

SOURCE: Adapted from H. N. Eisen, 1990, Immunology, 3rd ed., Harper & Row Publishers.

*The sensitivity depends upon the affinity of the antibody as well as the epitope density and distribution.

[†]Note that the sensitivity of chemiluminescence-based ELISA assays can be made to match that of RIA.

SOURCE: Adapted from N. R. Rose et al., eds., 1997, Manual of Clinical Laboratory Immunology, 5th ed., American Society for Microbiology, Washington, D.C.

MONOCLONAL ANTIBODY

ABO blood types **TABLE 6-2**

Control: No antibody present (ligand equilibrates on both sides equally)

(b) Heterogeneous antibody

labeled antibody to mAg

labeled anti-isotype antibody

labeled protein A

Перенос антигенов в буферном растворе

Влажный или полусухой перенос антигенов на мембрану

Figure 7. Semi-dry transfer system.

How it Works

- Traditional western blotting takes a variety of formats and reagent conditions to accomplish. It's a passive process!
- SNAP i.d. actively drives reagents through the membrane to increase the quality of the blots and increase the speed of immunodetection!
- **• It's a combination of reagent flows and concentrations**

Vs.

Standard 'rocking' of reagents

Actively drive reagents with vacuum flow

How it Works – reagent flows

Reagents penetrate more of the membrane 3D structure where the proteins are blotted.

Result = Increase quality of the blot in a SNAP!

Vacuum

SNAP

 \bullet \bullet \bullet

Standard vs. SNAP i.d. **concentrations**

Concentrations

- Blocking concentrations are limited to prevent clogging of blot holder
- Antibody concentrations are increased to speed up reaction kinetics

Compatible Blocking Reagents and Recommended Concentrations

How it Works – reagent flows

Blocking

- Efficient coverage of membrane which yields higher sensitivity
	- Can use 1/10th-1/100th less concentrated blocking solution to minimize overblocking
- Actively driven vacuum flow coats inner surfaces of membrane in 20 sec

Standard

Fig. 8. The surface topography of PEP (right) and Imm 2 (left). Images are for 3 µm squares obtained by atomic force microscopy in the Tapping Mode. Note that the maximum surface height depicted (Z axis) is 175 nm for Imm 2 but 300 nm for PEP. From Butler et al. (4).

Table 2 Adsorption-Induced Conformational Change

Fig. 1. The diffusion dependence of solid-phase immunoassay and methods used to reduce its influence. (A) The effect of vortexing (shaking) microtiters wells on establishment of equilibrium (from ref. *13***). (B) Illustration of the physical effect of vortexing microtiter wells (rotary agitation) on the distribution of the fluid phase relative to the solid phase. The fluid phase is depicted by wavy lines. (C) Alternative methods of confining the reaction volume to within close proximity to the solid**

Fig. 1. ELISA microarray immunochemical assay using the reaction of horse radish peroxidase (HRP) with tyramide for signal amplification.

Fig. 2. Sandwich assay developed for the renewable microcolumn sensor detection of botulinum toxin. It consists of a streptavidin-coated Sepharose 4B bead that is functionalized with a biotinylated AR1. This material is used to pack a microliter sized column capable of binding the surrogate botulinum toxin fragment. Once bound to the column the toxin fragment binds a secondary antibody (3D12) labeled with a fluorescent reporter.

Fig. 4. Calibration curves for the detection of BoNT/A-Hc fragment in buffer using an ELISA protein microarray. Assays were performed as described in Section 2 with the four capture antibodies used as shown in the figure legends. Each point represents the average of five microarray spots. (A) Standard assay incubation times were used. (B) Decreased detection antibody incubation time. (C) Decreased antigen incubation time, as indicated in the text.

 $14 \text{ fM} (1.4 \text{ pg m} L^{-1})$

Table 1

Comparison of reported limits of detection (LOD) of HRP with fluorescent substrates

Reference	Substrate	Reported LOD	LOD (moles of HRP)
$[13]$	Tyramine	0.1 mU	2.3×10^{-14} mol
[13]	Homovanillic acid	0.5 mU	1.1×10^{-13} mol
[4]	MHPMC	0.5μ mol	5×10^{-19} mol
$[2]$	p -Hydroxyphenylpropionic acid	$7.8 \mu U$	6.5×10^{-16} mol
$[2]$	Tyrosol	15.6 µU	1.3×10^{-15} mol
$[2]$	Tyramine	0.5 mU	4.2×10^{-14} mol
$[2]$	Homovanillic acid	1 mU	8.3×10^{-14} mol
[14]	o -Phenylene diamine	$0.56 \mu U$ ml ⁻¹ (2 ml)	1.1×10^{-16} mol
$[15]$	Amino aluminum phthalocyanine	0.6 pM $(10$ ml)	6×10^{-15} mol
[5]	DCM-OPA	\sim 20 pM (5 ml)	1×10^{-13} mol
	Lumigen PS-1	10^{-14} M	$< 10^{-18}$ mol
	Compound 4	4.6×10^{-14} M	4.6×10^{-19} mol

MHPMC, N-methyl-N-(4-hydroxyphenyl)methyl carbamate; DCM-OPA, N,N'-dicyanomethyl o-phenylenediamine.

Figure 1. Gold-silica nanoshells tuned to NIR wavelengths. Gold nanoshells are synthesized using SiO₂ cores (~114 nm diameter) with surface seeding using 1-3 nm gold particles on cores, followed by controlled surface fill-in with gold by reductive deposition from a gold salt solution. (a) The experimental and theoretical extinction spectra of nanoshells with [r1, r2] = [57,70] nm (inset). The radii define the inner and outer diameters of the shell and hence its thickness, leading to the generation of gold nanoshells with an absorption maximum in the NIR (~780 nm). (b) Scanning electron micrograph of synthesized gold nanoshells. Bar = 100 nm.

"http://www.ece.cmu.edu/~mems/pubs/show.php?pub_id=160

Fig. 1 (a) Size-dependent PL color and (b) schematic presentation of size, color, and PL wavelength of CdSe-ZnS QDs. (c) Absorption (solid lines) and PL (broken lines) spectra of CdSe QDs with various sizes. Reprinted with permission from Refs. [7] (a) and [30] (b). Copyright (1997, 2001) American Chemical Society

Методы коньюгации – иммобилизации антител

на квантовых наночастицах

Иммунофлюоресцентный анализ среза ткани с использованием антител, меченных квантовыми наночастицами

Fig. 1. Schematic view of a surface plasmon resonance (SPR) detector as utilized in a Biacore system. SPR arises when light is totally internally reflected from a metal-coated interface between two media of different refractive index (a glass prism and solution). If the incident light is focused on the surface in a wedge, the drop in intensity at the resonance angle appears as a "shadow" in the reflected light wedge, which is detected by a position-sensitive diode array detector. When an interaction between an immobilized ligand (e.g., an antibody, Y) and an analyte in solution (filled circles) occurs, the "shadow" is shifted on the detector, i.e., the angle θ changes.

Fig. 2. Immobilization of proteins to a gold surface using 3,3'-dithiodipropionic aciddi(N-succinimidylester) (DSP).

Биотинилированные антитела против токсина

Чиповая технология с использованием сандвич варианта ИФА и стрептавидин биотиновой ститемы

- *• Иммобилизация первых антител на чип, предпочтительнее ориентированная посадка антител*
- *• Захват антигена (зеленые шарики) антителами*
- *• Вторые специфические антитела,*
- *биотиновых комплексов*
- *спектрофотометрически*

888888888

 $\mathbb A$

A

Структура нейротоксинов клостридий и молекулярные мишени

Претеолитическое расщепление

А. $Zn/$ Light proteolytic Chain cleavage

Молекула токсина предшественника

Двуцепочная молекула токсина в активной форме

Созревание токсина и переход его в активную форму

Молекулы - мишени бактериальных нейротоксинов клостридий

Синаптические визикулы

Нейрональная мембрана

Олигонуклеотидные праймены

Липосомы-ПЦР иммуноанализ биотоксинов

Схема иммунохроматографического анализа

Figure 1. Schematic illustration of the principle of the one-step, noncompetitive FRET immunoassay for morphine. Eu-labeled antimorphine and Cy5-labeled anti-IC Fab fragments are added into a saliva sample. FRET occurs only when two fluorophores are close to each other; i.e., anti-IC Fab is specifically bound to IC. The star represents the analyte, and dotted patterns represent variable regions of the Fab fragment.

Figure 3. Cross-reactivity of the anti-morphine M1 Fab to codeine and heroin in a competitive ELISA. M1 Fab with various amounts of morphine, codeine, or heroin in PBS was added into morphine-BSA coated wells. After washings the bound Fab was detected with alkaline phosphatase conjugated anti-Fab antibody.

MILLIPORE

100 вариантов окраски сфер

MILLIPORE

Процесс детекции

Мультиплексный анализ технология Люминекс

Table 2 Adsorption-Induced Conformational Change

Phospholipid polymer brush to reduce unnecessary loss of bioactivity Improved binding capacity (1.8 antigens/antibody)

Retained binding affinity $(K_d \sim 10^{-10} / M)$

Table 1. Cooperative Index (n) and Dissociation Constant (Kd) of Antigen-Antibody Reaction

Conjugated to the amino group carrying platform using tyrosinase. To assess the orientation of immobilized antibodies, antigen binding capacity was measured with four di ere antantigen shaving molecular weight sranging from 66 to 330kDa. Forsmall antigens like albumin and CRP, highly oriented antibodies recorded as much as 1.8 (0.1 antigens per each immobilized antibody suggesting that at least 80% of immobilized antibodies reacted with two antigens. The multivalent binding analysis revealed that the oriented antibodies showed exceptionally strong a?nity for -10 antigens (Kd =8.6 10 mol/L). This value was 100-fold stronger than values for the partially oriented and randomly oriented antibodies and is comparable to the reported Kd values of the active antibodies. Bystrictlycontrolling orientation on an Antibiofoulingphospholipid platform, we have demonstrated that antibodyorientation improves the binding a?nity and the binding capacity of immobilized antibodies.

Fig. 2 The intrinsic properties of DNA molecules can be used to improve almost all fields of immunoassays. The scheme summarizes the range of different targets studied by exemplary applications including IPCR with protein chimeras.^{20,21} Universal-IPCR,¹² immuno-RCA,²⁵ PD-IPCR,⁴⁴ Imperacer^{vu},^{12,43} competitive assays for small molecules¹³⁴ or proximity ligation.⁴²

Fig. 1 Key steps of DNA-enhanced immunoassays. Note that additional details regarding antibody-DNA coupling are summarized in (Fig. 3) while aspects regarding signal-generation and DNA detection are further illustrated in (Fig. 6 and 7).

The nanostructured conjugates form the basis of powerful reagents for IPCR assays.

The evolution of immuno-PCR (IPCR): (A) the set-up of ELISA and IPCR is similar.

Instead of an enzyme marker, such as alkaline phosphatase (left), IPCR uses amplification of attached DNA for signal generation (right). (B) Different strategies for coupling antibodies and DNA: in the initial version of IPCR2 a Streptavidin (STV)–protein A chimeric fusion protein was used for tagging the detection antibody with biotinylated DNA (I). In the universal IPCR protocol, the signal generating complex is assembled in situ by subsequent incubation steps of biotinylated detection antibody, (strept-)avidin and biotinylated DNA; either using a non-biotinylated primary and a species specific secondary antibody (II) or a directly biotinylated primary antibody (III). The introduction of pre-assembled antibody–DNA conjugates takes advantage of either species- or marker-specific secondary conjugates92 (IV) or direct conjugation of target-specific antibodies and DNA14 (V). Approaches such as phage display mediated IPCR,44 tadpoles of antibodies and DNA,38 or native chemical ligation introduce elegant ways of coupling antibodies and DNA by circumventing artificial modifications such as biotin and complex crosslinking chemistries (VI). The linkage of multiple antibodies and DNA molecules with particles, as used in the bio-barcode technology92 has led to polyvalent reagents, which allow one to connect single antibody–antigen binding events to a larger number of DNA markers (VII). (C) Comparison of the multiple steps required for the in situ stepwise reagent assembly of the classical universal IPCR approach with the simplicity of specific antibody–DNA conjugates. Note that each coupling step requires optimization of reaction parameters and leads to a loss in sensitivity.

Typical results of immuno-PCR (IPCR) experiments. (A) Comparison of IPCR, the

analogous conventional ELISA for the detection of Rotavirus antigens.108 Note the high linearity and broad dynamic range of IPCR. (B) Comparison of different IPCR assay techniques for the detection of human TNFa: the use of target-specific antibody–DNA conjugates enables an increased sensitivity. The dark and light blue bars represent signals obtained by sequential IPCR (see Fig. 3B III) and direct IPCR with pre-assembled antibody– DNA conjugates (see Fig. 3B V), respectively. The red curve represents signals obtained in the analogous ELISA.

Lower limit of detected molecules in IPCR applications

Statistical analysis of references reporting DNA-enhanced immunoassays: (A) summary of detection limits reported. The majority of examples revealed a maximum sensitivity in the 0.016 amol–16 amol range (1000–100 000 molecules, respectively), thus

defining the standard performance of the method. Note that the broad detection range of about ≤10 molecules2,74,102 or single cells18 up to 1010 molecules in all cases involves a significant improvement of the analogous ELISA.137,138 A typical LOD is found at approx. 1000 olecules/sample, which is in accordance with the expected theoretical kinetics of immunoassays.13 (B) Overview of the N-fold improvement of conventional ELISA by the analogous IPCR. The sensitivity enhancement varies from 5-fold31 to up to 1 000 000 000- fold82,86 depending on the design and optimization state of the assay as well as the performance of the antibodies. The majority of studies reported a 100–1000-fold improvement in LOD. (C) Overview of the linear dynamic range of IPCR applications. While conventional ELISA typically reveals a dynamic range of two orders of magnitude in antigen oncentration, IPCR shows a significantly broader dynamic range (see also Fig. 5). In the majority of IPCR applications, the dynamic range comprised about four orders of magnitude.

Comparison of the most prominent methods for the detection and quantification of DNA amplicons generated in DNA-enhanced immunoassays. (A) Intercalation fluorescence markers with increased specificity for double-stranded DNA, such as ethidiumbromide or SYBR greenTM, are used in gel-electrophoresis or real-time PCR analyses. Note that for multiplex IPCR, it is necessary to separate amplicons of different length by gel-ectrophoresis while multiplex real-time detection can not be performed using intercalation marks. (B) Different types of sequence-specific fluorophore-labeled nucleic acid probes, e.g. TaqManTM or ScorpionTM are typically used for real-time quantitative PCR. During elongation of primers, the probes are modified and thereby, a fluorescent signal is generated. (C & D) Hybridization assays for sequence-specific DNA-detection. Sensitivity can be increased by binding of multiple fluorophores to the amplified DNA by means of hybridization of fluorophore-labeled probes to

products of RCA (C) or PCR (D) processes. In the case of immuno-RCA, the antibody–DNA–conjugate remains intact during DNA amplification and thus, a multitude of hybridization probes can bind to spots of microarrays, containing the immobilized antigen. In PCR-ELOSA

(D), hapten-labeled amplicons, generated during PCR, are immobilized by means of surface-bound capture oligonucleotides and subsequent detection is carried out by using hapten- specific antibody–enzyme conjugates.

is analyzed individually by a target specific assay.

Fig. 1. Schematic representation of immuno-PCR assay (A), and detection of protein A from S. aureus by immuno PCR (B).

and development in behalf sized from 1993. In our distribution of all of a state of the state of

Schematic representing the flow of reactions involved in the immuno-PCR signal amplification assay for detection of SEA and SEB. The Bead Retriever facilitated recovery of magnetic beads during chemical reactions and SE recovery during the assays.

water as a sample, and a blank well with PCR reagents only. Inset shows overlapping melting curves of amplified products of all PCR-positive samples.

(SEB). (B) Detection of SEB after incubation with S. aureus ATCC 14458 (SEB) using anti-SEB–coated magnetic beads. Control assays were performed with ATCC 13565 (SEA). Insets show melting curves of amplified by-products obtained with a real-time PCR.

Spiked conce (ng/ml or g)	Milk		Cream pie		Tuna salad		Ground turkey	
	Detected	C_T (cycles)	Detected	Cr (cycles)	Detected	C_T (cycles)	Detected	Cy (cycles)
SEA								
7.5.		26		28	NA		÷	27
0.75		27	NA'		NA			27
0.075		28		29	NA			28
0.0075''		29	NA		NA			29
0.00075		30		$30\,$	NA			30
0.000075		30	NA.		NA			31
0.0000075"		31	÷	$\overline{31}$	NA			32
SEB					130 July 1			
7.5.		23	NA			26	÷	22
0.75		24	NA		NA		÷	21
0.075		25	ΝA			27		23
0.0075''		26	NA.		NA			24
0.00075		26	NA		÷	30		25
0.000075		27	ΝA		NA			26
0.0000075"		28	NΑ			32		27

TABLE 2. iPCR-SA detection of SEA and SEB spiked in foods"

" C_T , threshold cycle. The control samples for no antigen, no primary antibody, no secondary antibody, no sample, and blank were negative for all samples tested (i.e., $C_T > 40$).

 32

NA

¹ NA, not assayed.

' Equivalent to 7.5 pg/ml or g.

 4 Equivalent to 7.5 fg/ml or g.

* Milk was heated in an autoclave at 15 psi.

 $^{\rm b}$ Equivalent to 7.5 fg/ml or g.

TABLE 4. Comparison of sensitivity of iPCR-SA assay with that of several commercial kits for detection of SEA and SEB diluted in TSB

 \overline{a} From TECRA.

^b From Toxin Technologies.

× Equivalent to 7.5 pg/ml or g.

 4 Equivalent to 7.5 fg/ml or g.

Figure 4. OS-ELISA using purified MBP-V_L and HRP-MBP-V_H of D11. Average of three measurements with 1 SD is shown. (A) A representative dose-response curve. Open and closed circles represent values with and without immobilized antihuman kappa chain antibody, respectively. (B) Cross reactivity with T3. Free T4 and T3 were incubated with HRP-MBP-V_H in the plate immobilized with MBP-V_L. V_L- shows the value without immobilized antibody. (C) Estimation of total T4 in serum using MBP $-V_L$ and HRP $-MBP-V_H$.

